# Heat storage in upper and lower body during high-intensity exercise in athletes with spinal cord injuries

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### **Abstract**

**Background:** The thermophysiology of athletes with spinal cord injuries (SCI) is not well understood. Spinal cord lesions impact muscle mass, thermoregulatory neural signals and circulatory function. Understanding SCI thermoregulation physiology would benefit exercise function. Therefore, this study was designed to describe heat storage in the upper and lower bodies of SCI and able-bodied (AB) athletes.

**Procedure:** Seven SCI and 8 AB athletes (matched for arm-crank  $VO_2$  peak) performed a ramp protocol in an environment similar to an indoor competitive environment (21°C±1.5°C, 55±3% relative humidity).

**Results:** SCI athletes experienced similar upper-body heat storage of  $0.82\pm0.59~\text{J.g}^{-1}$  and lower-body heat storage of  $0.47\pm0.33~\text{J.g}^{-1}$  compared with that of AB athletes at  $0.80\pm0.61~\text{J.g}^{-1}$  and  $0.27\pm0.22~\text{J.g}^{-1}$  for upper and lower body, respectively. There were no significant differences between groups for rectal temperature ( $T_{\text{rec}}$ ) or oesophageal temperature ( $T_{\text{es}}$ ). However, mean skin temperature ( $T_{\text{sk}}$ ) was significantly higher for SCI throughout the exercise bout (p=0.006).

**Conclusions:** The results of this study suggest that SCI and AB athletes appear to thermoregulate in a similar manner, though SCI tend to store slightly more heat.

# Introduction

Research on heat storage differences between the upper body and lower body for paraplegic athletes is sparse. However, a few stud-

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Fax: 509-963-1848 E-mail: pritcher@cwu.edu ies have reported heat storage when evaluating the effectiveness of various cooling interventions. Webborn  $et\ al.^1$  examined the effects of two cooling strategies (pre-cooling and cooling during exercise) on thermoregulatory responses of tetraplegic athletes. The authors, using a repeated measures design, examined two strategies during 28 minutes of intermittent arm crank exercise. The authors reported no difference (p=0.39) in heat storage between a control trial (3.62±0.4 J.g $^{-1}$ ) and either intervention during pre-cooling (4.17±0.4 J.g $^{-1}$ ) and cooling during exercise (3.15±0.35 J.g $^{-1}$ ).

Price and Campbell<sup>2</sup> examined upper- v. lower-body skin temperature in paraplegic athletes. Results from arm ergometry exercise indicated that paraplegic athletes (v. able-bodied athletes), showed lower skin temperatures for the lower body after 90 minutes of work at 80% of peak heart rate (HR) in room temperature. However, upper-body skin temperature was also lower for the paraplegic group v. the able-bodied group. The authors speculated that this could be due to atrophied musculature and/or an atrophied vascular system below the level of lesion.<sup>2</sup> Unfortunately no information was provided on rectal or oesophageal temperatures (two accepted measures of core body temperature), so heat storage cannot be calculated for the upper-body and lower-body regions. Furthermore, no effort was made to match groups for fitness.

In general, paraplegics seem to adequately regulate body core temperature at rest; however, they show a greater increase in core temperature when compared with able-bodied (AB) subjects during exercise and/or working conditions work. Furthermore, it has been demonstrated that individuals with a T6 (thoracic) lesion and below are subjected to smaller increases in core temperature than those individuals with a lesion above T6. These individuals, in turn, demonstrate smaller increases than those with tetraplegia (cervical lesions). Individuals with a spinal cord injury at or above T6 are prone to episodes of autonomic hyperreflexia when exposed to incompensable stimuli. These responses have been well documented by Jacobs and Nash, who further suggest that a common stimulus amongst others is a sudden rise in core temperature.

There seems to be a lack of knowledge regarding heat storage differences between upper-body (HS <sub>upper</sub>) and lower-body (HS <sub>lower</sub>) regions over the period of an exercise bout, particularly in spinal cord injured athletes (SCI) athletes. Understanding the heat storage of SCI athletes will illuminate both the thermal physiology as well as the circulatory function of this group. Furthermore, enhancing the knowledge of thermal physiology within this cohort could aid in the development of more effective cooling interventions. For example,

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the lower skin temperatures in SCI participants reported by Price *et al.*<sup>6</sup> may reflect a higher core temperature and reduced cutaneous vasodilatation, suggesting less effectiveness of skin cooling. A reduction in skin cooling has recently been noted by Pritchett *et al.*, where the authors highlighted a decrease in sweat response among participants with SCI, which led to a decreased ability to thermoregulate. This study therefore proposes to describe the heat storage dynamics over the course of a ~35-minute graded exercise bout under simulated gymnasium playing conditions (20°C±1°C; 45 -65±0.1% relative humidity) in both SCI and AB participants.

# Method Participants

Fifteen volunteers gave their informed consent to participate in this investigation, which had received approval by the University of Alabama Institutional Review Committee. The group was comprised of 7 paraplegic athletes (SCI) and 8 AB upper-body trained athletes (see Table I).

AB athletes were wheelchair basketball team members absent of SCI (N=4), and the remainder (N=4) were from the university swimming team.

Based on an alpha level of 0.05 an effect size of 1.0, a SD of 0.5 Jxg<sup>-1</sup> for heat storage, and a power of 0.80, an *a priori* power analysis indicated 7 subjects would be needed.<sup>8</sup>

#### **Exercise tests**

Participants visited the laboratory on two separate occasions. On the first occasion, volunteers performed an incremental arm-crank exercise (ACE) test to determine VO<sub>2</sub> peak with gas exchange indices collected using a Vacumed Vista mini cpx metabolic measurement system (Vacumed, Vista, CA). This involved two 5-minute submaximal exercise stages of arm-crank exercise (30 W and 50 W) separated by 1 minute of passive recovery. Once the two submaximal

mal ACE stages and a rest stage had been completed, volunteers exercised to volitional exhaustion at a ramp rate of 20 W every 2 minutes from an initial level of 110 W. All tests were conducted on a cycle ergometer (Monark 850E, Varberg, Sweden) adapted for upper-body exercise. Participants were instructed to maintain at least 50 rev. min<sup>-1</sup> throughout the test. For the second laboratory visit the exercise test consisted of multiple stages, beginning at a workload of 35 W. Resistance of each stage was held constant for 7 minutes. At the end of each stage, participants had a 1-minute passive recovery. The workload of each stage increased by 35 W, until such time that heat production exceeded heat dissipation as evidenced by a sudden increase in the time-slope of the T<sub>es</sub>. The increase in T<sub>es</sub> was identified as critical when it was greater than 0.2°C<sup>-1</sup> per minute. Temperature measures were conducted during the second laboratory visit only.

#### Temperature measures

On arrival at the laboratory for the incremental test, thermocouples (Physitemp Instruments INC., Clifton, NJ, USA) were positioned for measurement of rectal (Trec) and oesophageal temperatures (Tes). The oesophageal thermocouple was inserted with the following procedure. The inside of the nose of the subject was swabbed with a mild anaesthetic jelly (7.5% Benzocaine), and a light covering of jelly was also placed on the distal end of the thermistor. A single spray of a topical anaesthetic (Cetacaine, 14% Benzocaine, Cetylite Ind., Pennsauken, NJ USA) was sprayed on the back of the throat. After 2 minutes, the volunteers advanced the oesophageal probe through the nose and to the pharynx. At this point the probe was withdrawn slightly, and the volunteer was then requested to drink water through a right-angle straw and at the same time the probe was advanced into the oesophagus to a length of one-fourth of the volunteer's supine height and then taped to the nose and across the shoulder. A flexible rectal thermocouple (T<sub>rec</sub>) probe was self-inserted ~8 cm beyond the anal sphincter. The rectal probe was securely taped, and

TABLE I. Anthropometric and physiological measurements (means±SD) for able-bodied (AB) and spinal cord injured (SCI) participants (level of lesion and completeness of injury presented for SCI)

SCI (N=7)							AB ( <i>N</i> =8)					
Subject	Age	Height (cm)	Weight (kg)	Injury level	VO <sub>2</sub> peak <sub>-1</sub> I.min	Body fat (%)	Subject	Age	Height (cm)	Weight (kg)	VO <sub>2</sub> peak I.min	Body fa
1	23	170	60.0	T12/L1	2.06	25	1	21	185	73.0	3.20	14
2	31	174	44.5	T5 Com- plete	2.02	36	2	29	179	77.0	2.90	12
3	23	189	65.8	T11 Complete	2.89	10	3	23	198	93.0	4.10	16
4	19	174	57.0	T12 Complete	1.95	12	4	28	165	70.0	2.38	23
5	26	172	54.4	T6 In- complete	2.93	13	5	23	152	69.0	1.98	32
6	20	157	44.4	T3 Com- plete	1.81	18	6	38	155	64.0	2.04	20
7	26	176	51.0	T11 Complete	2.60	27	7	24	160	66.0	2.50	25
							8	38	153	48.0	1.90	13
Mean ±	24	173	53.9*		2.3	20		28	168	70.0	2.60	19
SD	4	9	7.9		0.5	10		7	17	12.7	0.80	7

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the thermocouple wire was passed over the back of the wheelchair to minimise interference with arm cranking.

Skin temperature  $(T_{sk})$  was continuously monitored from thermocouples placed at the following sites: forehead, forearm, upper arm, back, chest, thigh and calf. Thermocouples were attached to the skin using adhesive tape, cut around the head of the thermocouple, which held thermocouples in place without adding insulation.

Heat storage was calculated from the formula by Havenith *et al.* <sup>12</sup> Heat storage for the upper-body region was calculated using  $\Delta T_{es}$  and  $\Delta T_{sk}$  by tabulating the weighted mean skin temperature between forearm (20%), back (40%) and chest (40%). Lower-body heat storage was calculated using  $\Delta T_{rec}$  and  $\Delta T_{sk}$ , which was calculated using the mean skin temperature (thigh 70% and calf 30%) from the formula of Ramanathan. <sup>13</sup> Heat storage for each region was calculated where:

Heat storage =  $(0.8\Delta T_{rec} \text{ or } T_{es} + 0.2\Delta T_{skin}) \times C_b$ , where  $C_b$  is the specific heat capacity of body tissue  $(3.49J \times g^{-1} \times {}^{\circ}C^{-1})$ .

# Statistical analysis

Heat storage for the upper body (HS<sub>upper</sub>) and heat storage for the lower body (HS<sub>lower</sub>) were compared using paired t-tests. Level of significance was set at alpha $\leq$ 0.05. A one-way analysis of variance was used to compare the difference between SCI athletes and matched AB athletes. Furthermore, to allow for a depletion of subjects due to differentiated termination time, a harmonic mean was calculated and analysis over time using a repeated measures ANOVA with a Bonferroni  $post\ hoc$  test employed where necessary.

#### Results

Descriptive statistics (means and standard deviations) for SCI and AB are presented in Table I. There was no difference in absolute VO<sub>2</sub> peak, stature and age. However, body mass was significantly different between groups (p=0.03). AB athletes were matched to SCI athletes based on activity status, VO2 peak, with 3 of the 8 AB being active participants in college wheelchair basketball. Thermoregulatory responses during exercise for SCI and AB were compared and presented graphically. There was no significant difference (p=0.06) in Tes between SCI (38.0±0.2°C) and AB (37.6±0.4°C) (Fig. 1). However, it was noted that there was a greater increase in Tes for SCI within the last two stages of the exercise bout.  $T_{\text{rec}}$  (Fig. 2) for both groups were similar with no statistical difference between groups (p>0.05). Figures are reported with the sample size, as the increasing intensity lead to a depleted sample size as individual termination points were reached. One subject (T3 lesion level) completed two stages, and was matched with an AB subject that completed two stages. Only two subjects could not complete the final stage (90 W). Data are presented for all stages that more than 70% of the subjects completed. Analysis of variance indicated that mean skin temperature for the lower body (M<sub>sk</sub>) (Fig. 4) for SCI subjects was significantly higher than for AB throughout the exercise bout (p=0.006). However, mean skin temperature for the upper body (Fig. 3) was significantly different than for the first (30 W) stage (SCI: 35.2±0.9°C, AB: 33.4±0.8°C) and second stage (50 W) (SCI: 33.4±0.9°C, AB: 33.7±1.0°C). However, for the last two stages, there were no significant differences detected between groups. There was no significant difference observed between upper body and lower body for heat storage between SCI and AB athletes (p=0.38, Fig. 5). Furthermore, it is interesting to note that there was a significant difference observed between HS<sub>upper</sub> and  $HS_{lower}$  body for SCI (0.82±0.59 J.g<sup>-1</sup> and 0.47±0.33 J.g<sup>-1</sup>) (p=0.04) and also for AB (0.80 $\pm$ 0.61 J.g<sup>-1</sup> and 0.27 $\pm$ 0.22 J.g<sup>-1</sup>) (p=0.03). Heat storage for SCI and AB per stage for both upper and lower body are

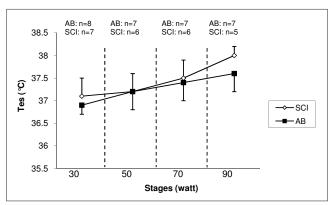


Fig. 1. Oesophageal temperature ( $T_{es}$ ) for SCI and AB athletes during incremental exercise for arm-crank ergometry. Sample size (N) is given for each stage that was completed.

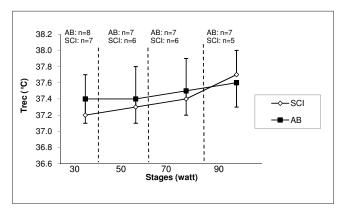


Fig. 2. Rectal temperature ( $T_{rec}$ ) for SCI wheelchair athletes and AB controls during incremental exercise for arm-crank ergometry. Sample size (N) is given for each stage that was accomplished.

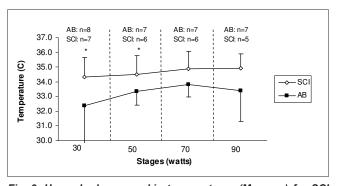


Fig. 3. Upper body mean skin temperatures (M<sub>sk-upper</sub>) for SCI wheelchair athletes and AB controls during incremental exercise for arm-crank ergometry. Sample size (N) is given for each stage that was accomplished.

presented in Figs 6 A and B, respectively. There was no significant difference for HS between stages for either group.

#### **Discussion**

The current study was undertaken in a common mild environment (simulation of a typical wheelchair basketball playing environment) under exercise conditions that were intended to simulate the duration and intensity of a typical competition half. Our intent was to maintain high ecological validity throughout the investigation in order to make the results of this study inferable to an active SCI population par-

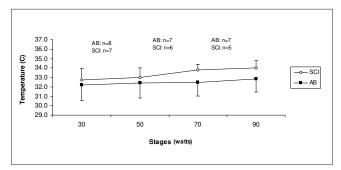


Fig. 4. Lower body mean skin temperature ( $M_{sk-lower}$ ) for SCI wheelchair athletes and AB controls during incremental exercise for arm-crank ergometry. Sample size (N) is given for each stage that was accomplished.

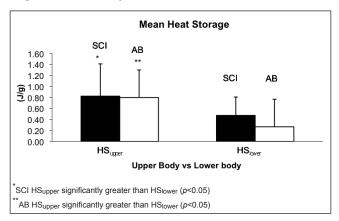


Fig. 5. Mean heat storage for SCI wheelchair athletes and AB controls during incremental exercise for arm-crank ergometry.

taking in wheelchair sports. It has been stated that individuals with SCI have a compromised ability to thermoregulate, which can lead to magnified risk of thermal injury. <sup>14</sup> The purpose of this paper was to add to the understanding of the thermophysiology of heat storage in SCI athletes.

All subjects were matched based on fitness. Three AB subjects had experienced training identical to the SCI group participating on the same wheelchair basketball team and swimming teams (absolute  $VO_2$  peak is presented in Table I). Buresh *et al.*<sup>15</sup> suggested body mass and heat storage in AB athletes are significantly correlated. However, it is difficult to match these two populations (SCI and AB) for body mass.

As heat storage is a composite of both core temperature and skin temperature changes, for this study heat storage was compared between upper and lower body. There were lower heat storage values for the lower body compared with the upper body for both groups. However, there was no significant difference between groups. Reduced heat storage for the lower body might have been due to the lack of muscular contraction in the lower body. Therefore, there was little metabolic heat production.  $HS_{lower}$  was comprised of  $T_{rec}$  and M<sub>sk</sub> (calf and thigh). There was no significant difference in the change in  $T_{\text{rec}}$  between the SCI and AB groups. This could account for little differences detected between the two populations. Both groups also demonstrated little difference for HSupper. Greater HS for the upper body observed for both groups might have been due to the nature of the exercise mode. It could also be speculated that due to the SCI athletes having a greater sweat response above their level of lesion. It has been demonstrated that at rest SCI athletes have warmer skin temperature, which enables an earlier onset of sweating, and

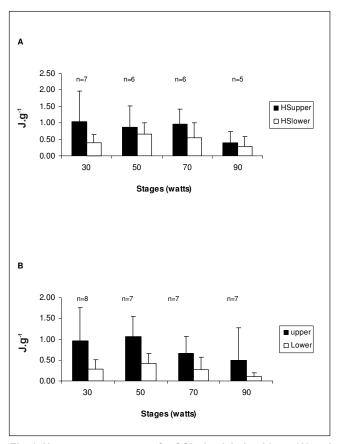


Fig. 6. Heat storage per stage for SCI wheelchair athletes (A) and AB controls (B) during incremental exercise for arm-crank ergometry. Sample size (N) of athletes that completed the stage.

therefore earlier skin cooling when compared with AB athletes. <sup>16</sup> This upper-body adaptation to an impaired thermoregulatory ability might help compensate for the lower body inability to dissipate stored heat.

 $M_{sk}$  temperature (Fig. 3) for the upper body was higher than the lower-body skin temperature in SCI. Also, SCI experienced higher mean skin temperature in both the upper and lower body than did the AB. This is in accordance with Fitzgerald  $et~al.,^{17}$  who noted that volunteers with SCI who performed prolonged exercise at 24 - 25°C experienced an increase of ~0.7°C (in core temperature). It was suggested that the increase in  $M_{sk}$  was due to heat being generated from the working muscles, which was then transferred to the skin. Heat from the insensate skin would not be able to be dissipated, thus this would result in an increase in skin temperature.

One of the more extensively compiled research composites is that of sweat response between AB and SCI individuals and between different levels of SCI.  $^{3,4,18}$  A reduction in whole-body sweating leads to greater increase in core temperature at rest, and a greater drive for sweating for a given environmental temperature.  $^{19,20}$  The current investigation reported slightly elevated  $T_{es}$  for SCI athletes initially  $(37.1\pm0.4\,^{\circ}\text{C})$  compared with AB  $(36.9\pm0.2\,^{\circ}\text{C})$ . Similar responses were recorded for  $T_{rec}$  (SCI =  $37.2\pm0.5\,^{\circ}\text{C}$  and AB =  $37.4\pm0.3\,^{\circ}\text{C}$ ). However, it could be noted that the fluctuation in  $T_{es}$  and  $T_{rec}$  could quite possibly be due to circadian variation or day-to-day variations. Trec was late to increase in the SCI athletes, only showing increase in the last two stages. This could possibly be due to a lag time experienced in Trec measures, where rectal temperature measures have been shown to respond more slowly.  $^{11}$ 

## Conclusion

In summary, the current study examined the heat storage response during upper-body high-intensity exercise. Results of this study suggest SCI and AB athletes were similar with respect to thermoregulation during arm cranking. SCI athletes tended to store slightly more heat in the lower body than AB athletes. Both groups also demonstrated little difference for heat storage in the upper body. Similarly, there was no significant difference observed for lower-body heat storage values. In a simulated gymnasium temperature environment it appears the matched groups demonstrated few meaningful differences in the current paradigm. Future research should look at more sophisticated observation of heat transfer like thermography to better understand the dynamics of stored heat within this population during high-intensity activity.

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